

## Treatment of Venous Malformations With an Intense Pulsed Light Source (IPLS) Technology: A Retrospective Study

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**Background and Objective:** The intense pulsed light source (IPLS) technology provides an innovative concept in the treatment of vascular lesions. We investigated the effectiveness of IPLS in the treatment of venous malformations.

**Study Design/Materials and Methods:** A retrospective study of 11 patients with venous malformations (VMA) treated with IPLS was initiated. Clinical VMA characteristics recorded were size and location. Data collected included treatment parameters (filters, pulse duration, fluence, and pulse sequencing), % clearance, and side effects (e.g., swelling, blisters, crusting, pain, altered pigmentation, and scarring).

**Results:** Good and very good (70–100%) clearance was achieved in 8 malformations smaller than 100 cm<sup>2</sup>. Especially small lesions needed only 2–3 treatments. Three VMA larger than 100 cm<sup>2</sup> could be cleared well in an average of 18 sessions. The most frequently used parameters were the 590 nm filter in long pulse mode, triple pulses, and fluences at an average of 80.4 J/cm<sup>2</sup>. Side effects included prolonged erythema in 23.6, swelling in 17.9%, crusting in 4.7%. Bleeding, hypo-, hyperpigmentation, and scarring were rare (0.9% respectively).

**Conclusion:** IPLS presents an effective method for treating VMA, especially small malformations, with a justifiable rate of side effects when optimal parameters are chosen. *Lasers Surg. Med.* 25:170–177, 1999. © 1999 Wiley-Liss, Inc.

**Key words:** PhotoDerm VL®; pulsed laser and light systems; venous malformations

Venous malformations manifest in a wide spectrum, from isolated cutaneous ectasias or a localized spongy mass, to a complex lesion involving multiple tissues and organs [1,2]. Possible complications of venous malformations are phlebothrombosis within a malformation, palpable, small thrombi with localized pain, or consumptive coagulopathy secondary to stasis, within the ectatic vascular channels. In the past, venous malformations could not usually be completely eradicated. Previous therapeutic modalities like excision, electrocoagulation, or sclerotherapy were accompanied by complications such as bleeding, pain, and scarring, or were limited by size and extension of vascular lesions [2,3]. In the last 15 years, several lasers such as the argon laser, the Nd:YAG (1,064 nm) laser, the KTP-

frequency doubled Nd:YAG (532 nm) laser, the copper vapour laser, or flashlamp pumped pulsed dye lasers were used. However, in the treatment of large venous malformations, these lasers were limited either by a lack of response or a high rate of side effects [4–15].

Alternatively to laser systems, PhotoDerm VL® is an innovative, intense pulsed light source (IPLS) that emits polychromatic, noncoherent light. This new device utilizes light beams that may be varied in terms of wavelength, pulse duration, and fluence. Thus vascular lesions of vari-

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ous depth and size (e.g., Spider nevi, telangiectasia, port wine stains, poikiloderma of Civatte) and hypertrichosis can be treated effectively [16–24]. Benign venous malformations seem to be a further interesting indication for the IPLS because of their deep seated, large vessels and cavernous structures.

Treatment of venous malformations in 11 patients was performed by using these principles during the current clinical study of IPLS.

## MATERIALS AND METHODS

From December 1994 to August 1998, 11 patients (seven female, four male) with 11 venous malformations were treated using an intense pulsed light source (IPLS) (Photoderm VL®, ESC-Sharplan Medical System Ltd., Haifa, Israel), emitting incoherent light with a wavelength continuum ranging from 515 to 1,000 nm. Depending on the characteristics of the lesion and the skin type, different filters (515, 550, 570, 590 nm) can be used which filter out shorter wavelengths. A single, double, or triple pulse can be administered. Pulse duration ranges between 0.5 and 25 ms in the short pulse mode and up to 30 ms in the long pulse mode. Fluence lies between 3 and 90 J/cm<sup>2</sup>. Delay time between pulses is adjustable from 10 to 500 ms. The rectangular spot exposes an area of 2.8 cm<sup>2</sup> (8 × 35 mm).

All patients with venous malformations (VMA) undergoing an IPLS therapy were included in this retrospective study (Table 1). The ages of the patients ranged from three to 61 years. Two patients were under the age of 12 (three and 10 years). Three of the treated VMA were localized on the face and neck, four on the trunk, two on the legs, and two on the penis. Eight lesions were smaller than 100 cm<sup>2</sup>; three VMA were larger than 100 cm<sup>2</sup>. In five patients, color-flow Doppler sonography of the vascular malformation was carried out before treatment to define depth and thickness of the vessel malformations (HDI 3000; ATL USA, Inc.; transducer CL 10-5 compact linear array Entos™, ATL USA, Inc.). The depth ranged between 0.5 and 2 cm; the thickness between 0.4 and 2 cm. Six (54.5%) of the 11 VMA had previously been treated without success by surgical excision, sclerosing, laser, cryotherapy or x-ray therapy. In five patients, among them two children, local anaesthetics (2.5% Lidocain–2.5% Prilocain-cream; 10% Lidocain-spray) were applied before each IPLS therapy. Immediately before the treatment, an approximately 1 mm layer

**TABLE 1. Patient Demographics**

|                        |                    |
|------------------------|--------------------|
| Number of patients     | 11                 |
| Male                   | 4                  |
| Female                 | 7                  |
| Age                    | 3–61 years         |
| < 12 years             | 2 (3 and 10 years) |
| Fitzpatrick skin type  | I 4                |
|                        | II 7               |
|                        | III —              |
|                        | IV —               |
| Size of VMA            |                    |
| < 100 cm <sup>2</sup>  | 8                  |
| > 100 cm <sup>2</sup>  | 3                  |
| Localization           |                    |
| Face                   | 2                  |
| Neck                   | 1                  |
| Trunk                  | 4                  |
| Legs                   | 2                  |
| Penis                  | 2                  |
| Previously treated VMA | 6                  |
| Local anaesthesia      | 5 patients         |
| (10% lidocain spray,   | (among 2 children) |
| 2.5% lidocain–2.5%     |                    |
| prilocain cream)       |                    |

of a clear, cooled waterbased gel (Coupling Gel; ESC) was placed between the emitting crystal and the skin to decrease epidermal heating. Following treatment, ice-cold refrigerant packs were applied to the area for 20–30 minutes to treat the sunburn-like discomfort and to prevent inflammatory swelling. When crusting occurred, an antibiotic ointment (3% Chlortetracyclin) was required. Patients were advised to avoid sun exposure during the whole treatment period. Patients were treated with IPLS in intervals of 1–8 weeks.

Due to the retrospective character of our study, no uniform parameters were employed. The filters used were 550, 570, and 590 nm, total fluence ranged from 32 to 90 J/cm<sup>2</sup>, and energy was applied in single, double, and triple sequential pulses.

Test patches were done. The fluences were raised corresponding to the appearance of adverse reactions and to lightening effect. Most of the lesions were treated twice over the same area (two passes per session), with the exception of the legs because of higher sensibility of the skin and poor lymphatic drainage there in comparison to other regions.

Photographs were taken under identical conditions. A Cannon EOS 100-camera with Agfa CTX 100 (Leverkusen, Germany) film was consistently used. Pre- and post-treatment photographs were evaluated by three physicians independently. The degree of clearance was determined.

Results were ranked into one of four categories: 85–100% clearance (very good), 70–84% clearance (good), and 50–69% clearance (fair), and less than 50% clearance (poor). The post-treatment presence or absence of prolonged erythema, swelling, blisters, bleeding, crusting, hypo- or hyperpigmentation, or scarring was recorded according to statements from the patients.

## RESULTS

### Venous Malformations < 100 cm<sup>2</sup>

A very good clearance could be observed in seven cases after two to nine treatments. Good clearance was shown in one malformation. It is noteworthy that two small lesions (1.5 and 4 cm<sup>2</sup>) only needed two and three treatments respectively, for 95% clearance (Fig. 1A,B). One VMA (with a thick nodular part) showed only 70% clearance after seven sessions (Table 2).

### Venous Malformations > 100 cm<sup>2</sup>

Treatment results for malformations larger than 100 cm<sup>2</sup> (n = 3) included three with good clearance. The average number of sessions in this group was 18 (Table 2; Fig. 2A,B).

### Treatment Parameter

The total number of sessions in 11 patients was 106. Initially, the 590 nm filter was used for deep vessels (n = 95; 89.6%); here most treatments were applied in the long pulse mode (n = 73; 76.8%). For superficial parts of the lesions, the 570 nm filter (n = 9; 8.5%) and the 550 nm filter (n = 2; 1.9%) were required. Most treatments were carried out in sequences of triple pulses (n = 75; 70.7%; especially for deep vessels). The pulse duration sequence 5.0–6.6–8.7 ms was most frequent for the long pulse mode; 3.8–3.1–2.5 ms for the short pulse mode. Double pulses (n = 29; 27.4%) and single pulses (n = 2; 1.9%) were also employed but less frequently (especially for superficial vessels). Fluences ranged from 32 to 90 J/cm<sup>2</sup>. The average fluency used in the short pulse mode was 50 J/cm<sup>2</sup>; in the long pulse mode 80.4 J/cm<sup>2</sup>.

### Side Effects

Side effects included prolonged erythema in 23.6% of treatment sessions (n = 25), persisting for a maximum of five days, typically 24–72 hours. Immediate post-treatment swelling lasting only some hours was common. Swelling persisting longer than 24 hours was observed in 17.9% (n =

19), blisters in 2.8% of sessions (n = 3). In 4.7% (n = 5), crusting was noted that resolved within 1–2 weeks. Prolonged post-treatment pain (longer than 12 hours) occurred six times (5.7%). Bleeding, hypo-, hyperpigmentation, and scarring were rare (n = 1; 0.9% respectively) (Table 3).

## DISCUSSION

Due to its specific way it works based on the principle of selective photothermolysis [25], the flashlamp-pumped pulsed dye laser (FLPDL; 577 or 585 nm) has proven itself an effective and safe method for treatment of various vascular lesions, e.g., port wine stains and initial hemangioma, over the past decade [26,27]. However, deep-seated vessels and cavernous malformations cannot be targeted successfully by the FLPDL beam because of its shallow penetration depth. Histologic studies demonstrated insufficient coagulation of dermal vessels below 1.16 mm in human skin [8,9,28]. With larger and deeper vessels, it is important to use longer wavelengths, longer pulses, and higher fluences. The IPLS utilizes a high energy flashlamp with variable wavelength spectrum, allowing the simultaneous application of longer wavelengths (515–1,000 nm). The concept of the IPLS is selective photothermolysis [29], as used in the dye laser. The target chromophore is oxyhemoglobin. Effective heating of the upper as well as deeper vessels could be obtained with the IPLS because of its wavelength spectrum [16]. Whereas the penetration depth increases at longer wavelengths, the absorption of laser energy in blood vessels decreases dramatically [30]. Concomitant increases in fluence are required to compensate for the decreased absorption and increased volume of blood being heated [11]. The IPLS allows for the application of high fluences in the so-called long pulse mode. With fluences of up to 90 J/cm<sup>2</sup>, larger volumes of blood, e.g., in VMA, are sufficiently heated. Consequently, the blood in the vessels and caverns coagulates, partly felt as fixed thrombosis and detectable by ultrasound sonography. The vessels are injured by selective photothermolysis which leads to their destruction, removal, and replacement by granulation tissue [31].

The FLPDL is less effective for large vessels or multi-layer vessels also because of its short pulse duration (450 μs). Ideally, the pulse duration should be compatible with the diameter of the vessel and be about equal to the thermal relaxation time for that dimension [32–34]. If the laser



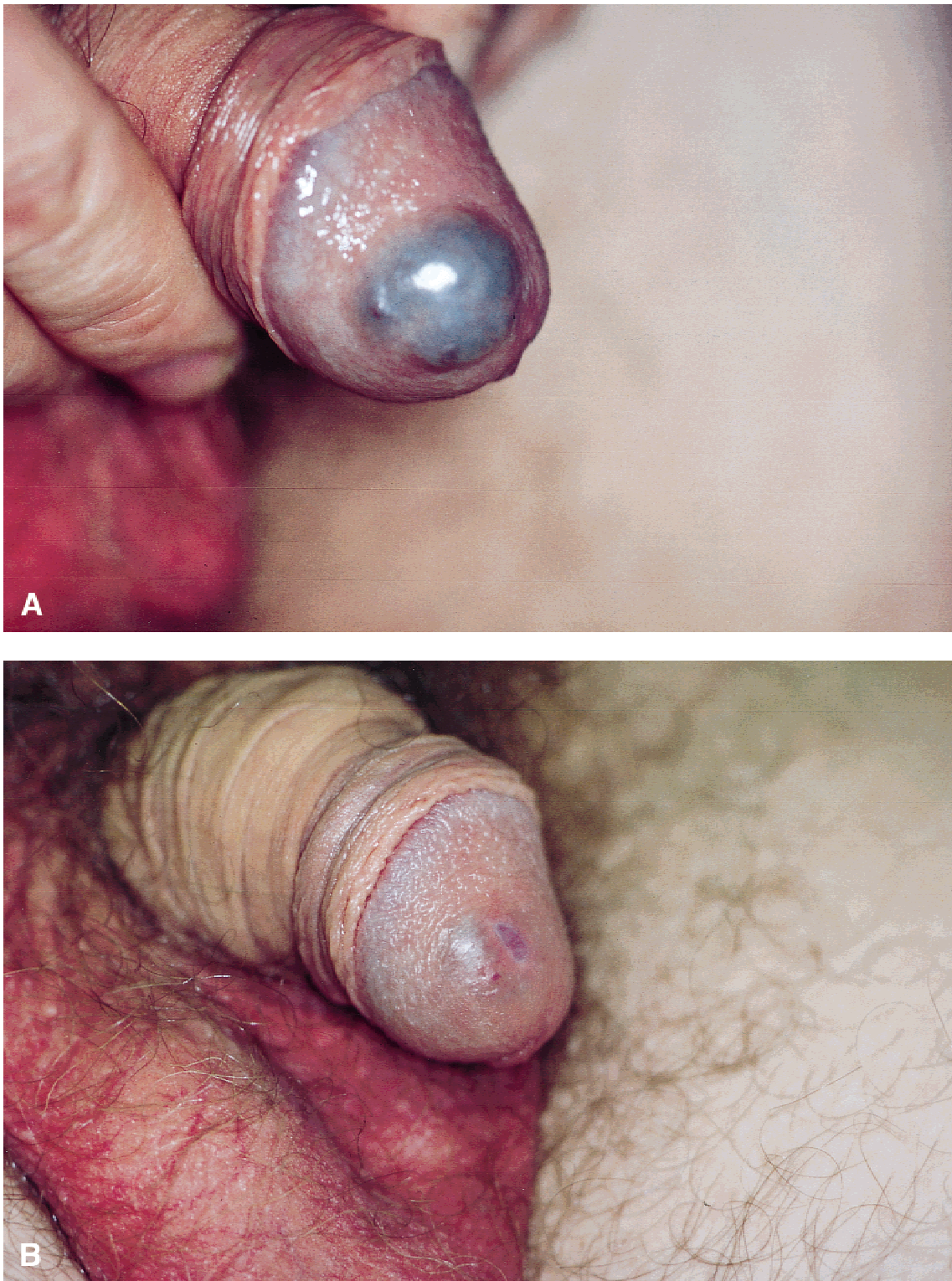


Fig. 1. **A:** A 35-year-old man with a small superficial venous malformation on the penis. **B:** A 95% clearance after two treatments with the PhotoDerm VL® with minimal textural change.

**TABLE 2. Clearance (%) of Venous Malformations After IPLS Therapy in Relation to the Lesion Size**

| Sessions<br>Size (cm <sup>2</sup> ) | 1 | 2  | 3  | 4 | 5 | 6 | 7  | 8   | 9  | 10 | 11 | 12 | > 12 |
|-------------------------------------|---|----|----|---|---|---|----|-----|----|----|----|----|------|
| 1.5                                 |   |    | 95 |   |   |   |    |     |    |    |    |    |      |
| 4                                   |   | 95 |    |   |   |   |    |     |    |    |    |    |      |
| 8                                   |   |    |    |   |   |   |    | 100 |    |    |    |    |      |
| 12                                  |   |    |    |   |   |   |    | 100 |    |    |    |    |      |
| 15                                  |   |    |    |   |   |   | 95 |     |    |    |    |    |      |
| 15                                  |   |    |    |   |   |   | 70 |     |    |    |    |    |      |
| 40                                  |   |    |    |   |   |   | 95 |     |    |    |    |    |      |
| 60                                  |   |    |    |   |   |   |    |     | 90 |    |    |    |      |
| 140                                 |   |    |    |   |   |   |    |     |    |    |    |    | 80   |
| 190                                 |   |    |    |   |   |   |    |     |    |    |    |    | 70   |
| 260                                 |   |    |    |   |   |   |    |     |    |    |    | 80 |      |

pulse duration is too short, heating will be confined to a thin superficial layer on top of the vessel during the laser pulse. This is likely to be insufficient to coagulate or thrombose the whole vessel [11]. In comparison to FLPDL, IPLS provides longer pulses (0.5–30 ms), and thus, sufficient high energy densities. The pulse duration of the IPLS flash ranges well below the thermal relaxation time of dermal cells, thus avoiding involvement and damage of the surrounding tissue. Traditional continuous wave (cw) lasers, such as the Nd:YAG (1,064nm) laser, have also been used to treat deep seated blood vessels, e.g., in subcutaneous hemangiomas [35–38]. However, the wavelength is absorbed by water and, to a certain degree, by melanin and hemoglobin. Therefore, as with the CO<sub>2</sub> laser, tissue damage is relatively nonspecific. Additionally, the cw mode causes an extended thermal damage zone. Thus, such adverse effects as scarring and textural or pigmentary changes were common [10,34,39].

Using IPLS, splitting light into double and triple pulses with delay times between 0.5 and 500 ms is possible. Thus, venous malformations or cavernous hemangioma can be treated effectively by additional heating [40–42]. This split light application ensures adequate cooling of the epidermis and dermis between the flashes.

The described innovative technical requirements of IPLS concur with our observations in this study. So that the deep venous vessel structure can be reached and effectively thermally damaged, the 590 nm cut-off filter and the long pulse mode with relatively high energy densities (average of 80.4 J/cm<sup>2</sup>) were most frequently used. Mostly triple pulse sequences with 5.0–8.7 ms pulses each were applied to protect the epidermis. With these parameters, we could achieve good results on our patients with venous malfor-

mations. In the course of this, the success of the therapy seems to also depend upon the size of the lesion to be treated. Venous malformations smaller than 100 cm<sup>2</sup> reached good to very good clearance after two to nine treatments. Eighteen treatments were needed for good clearance of lesions larger than 100 cm<sup>2</sup>. In the cases, treatment was continued until no further lightening was visible. The number of sessions for larger lesions appears high, however they were tolerated by the patients because a treatment with FLPDL had caused little or no lightening. Morelli et al. reported similar results in a study of the treatment of port wine stains with FLPDL; 32% of the patients with port wine stains smaller than 20 cm<sup>2</sup> showed 100% clearance in comparison with 8% of the patients with larger port wine stains [43].

Adverse reactions were predictable. In the current study, prolonged erythema and swelling were observed relatively often (23.6% and 17.9%, respectively). Blisters and crusting were predominantly in VMA with thick nodular parts. The utilization of higher fluences seems to cause epidermal damage due to scattering of light and conduction of heat from especially large vessels to the surrounding tissue. Transient changes in pigmentation, e.g., hypopigmentation or hyperpigmentation and scarring, were relatively infrequent (1 of 106, 0.9%, respectively). Juxtaposed results to the incidence of side effects were described in studies using IPLS. Although transitory adverse effects were rare in the Goldman/Eckhouse study [16] (blisters 2%, crusting 0.4%, hypopigmentation 3%, hyperpigmentation 4%), Green [44] observed a higher incidence of blisters (42%), hypopigmentation (20%), hyperpigmentation (50%) and scarring (21% vs. 0.5% in Goldman/Eckhouse study) using IPLS for treatment of leg telangiectases. In comparison, FLPDL caused post-purpura pig-

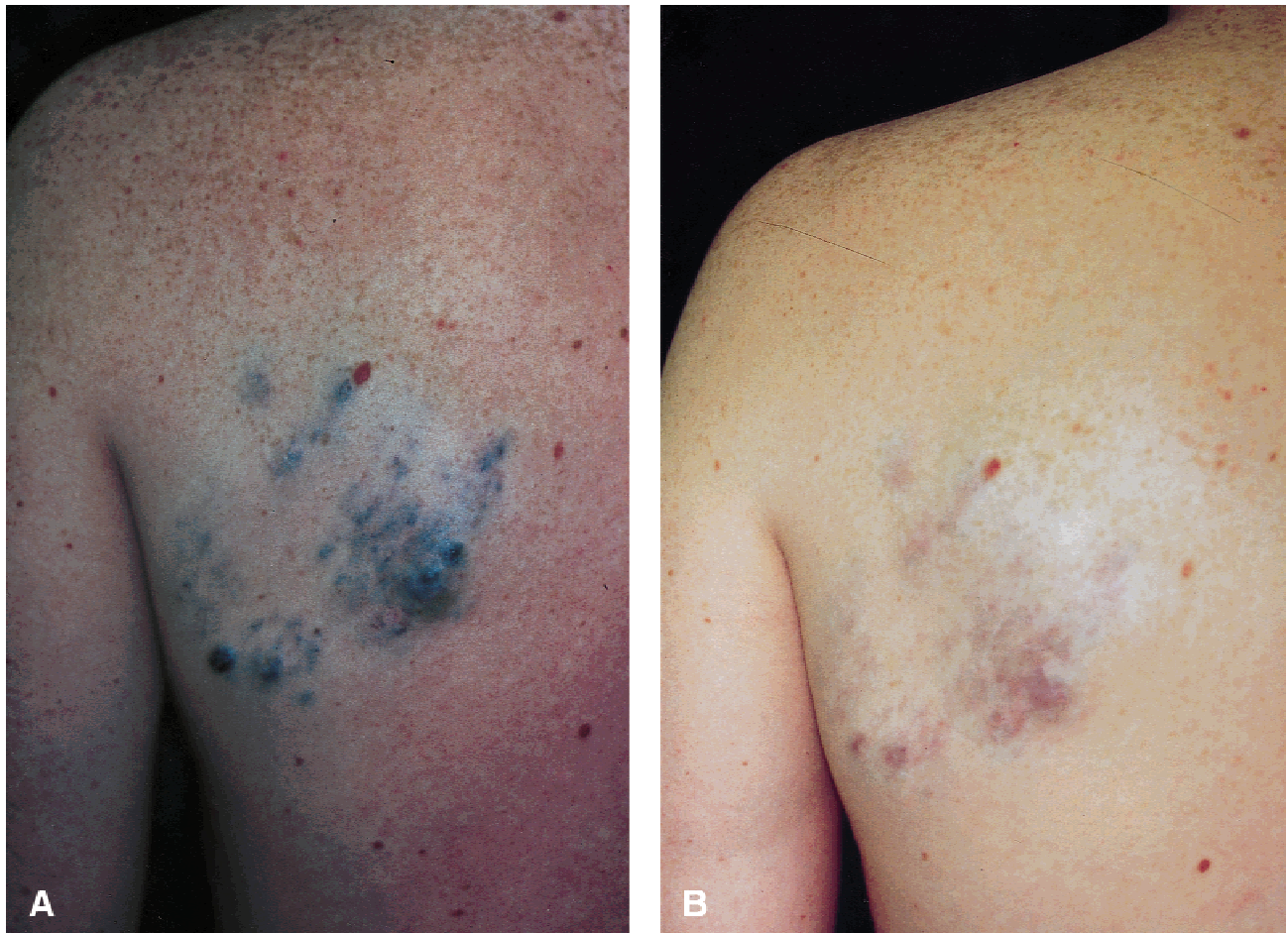


Fig. 2. **A:** A 31-year-old man with large and deep-seated (up to 2 cm under the surface) venous malformation on the left shoulder. **B:** Good (70%) clearance after 14 treatments with the PhotoDerm VL® with slight hypopigmentation.

**TABLE 3. Side Effects During Venous Malformation Therapy by IPLS**

| Side effects        | Appearance of side effects | (%) Total number of sessions (n = 106) |
|---------------------|----------------------------|--|
| Prolonged erythema  | 25                         | 23.6                                   |
| Prolonged swelling  | 19                         | 17.9                                   |
| Blisters            | 3                          | 2.8                                    |
| Crusting            | 5                          | 4.7                                    |
| Bleeding            | 1                          | 0.9                                    |
| Post-treatment pain | 6                          | 5.7                                    |
| Hypopigmentation    | 1                          | 0.9                                    |
| Hyperpigmentation   | 1                          | 0.9                                    |
| Scarring            | 1                          | 0.9                                    |

mentation reported at a frequency of 9 to 57% [9,34,45–48] and post-inflammatory hypopigmentation in 2% to 10% [34,47,49–51].

The success rate with venous malformations, combined with a relatively low incidence of side effects, makes IPLS a useful alternative for ad-

junctive or primary treatment of venous malformations. We think IPLS will find a firm place in the therapy of vascular lesions, especially venous malformations. However, what we have still awaits large, critical, and especially prospective clinical studies and, possibly, more refined treatment parameters.

## REFERENCES

1. Landthaler M, Hohenleutner U. Zur Klassifikation vaskulärer Fehl- und Neubildungen. *Hautarzt* 1997;48:622–628.
2. Fishman SJ, Mulliken JB. Hemangiomas and vascular malformations of infancy and childhood. *Pediatric Surgery* 1993;40:1177–1200.
3. Vente C, Menzel S, Rupprecht R, Günzl H-J, Neumann C. Sklerosierung bei multiplen familiären Glomangiomen. *Hautarzt* 1998;49:657–661.
4. Apfelberg DB, Bailin P, Rosenberg H. Preliminary inves-



- tigation of KTP/532 laser light in the treatment of hemangiomas and tattoos. *Lasers Surg Med* 1986;6:38–42.
5. Goldberg DJ, Marcus J. The use of the frequency-doubled Q-switched laser in the treatment of small cutaneous vascular lesions. *Dermatol Surg* 1996;22:841–844.
6. Pickering JW, Walker EP, Butler PH, van Halewyn CN. Copper vapour laser treatment of port-wine stains and other vascular malformations. *Br J Plast Surg* 1990;43:273–282.
7. Derby LD, Low DW. Laser treatment of facial venous vascular malformations. *Ann Plast Surg* 1997;38:371–378.
8. Fiskerstrand EJ, Svaasand LO, Kopstad G, Ryggen K, Aase S. Photothermally induced vessel-wall-necrosis after pulsed dye laser treatment: Lack of response in port-wine stains with small sized or deeply located vessels. *J Invest Dermatol* 1996;107:671–675.
9. Hohenleutner U, Hilbert M, Wlotzke U, Landthaler M. Epidermal damage and limited coagulation depth with the flashlamp-pumped pulsed dye laser: A histochemical study. *J Invest Dermatol* 1995;104:798–802.
10. Hellwig S, Petzoldt D, König K, Raulin C. Aktueller Stand der Lasertherapie in der Dermatologie. *Hautarzt* 1998;49:690–704.
11. Hsia J, Lowery JA, Zelickson B. Treatment of leg telangiectasia using a long-pulse dye laser at 595 nm. *Lasers Surg Med* 1997;20:1–5.
12. West TB, Alster TS. Comparison of the long-pulse dye (590–595 nm) and KTP (532 nm) lasers in the treatment of facial and leg telangiectasias. *Dermatol Surg* 1998;24:221–226.
13. Adrian RM, Tanghetti EA. Long pulse 532-nm laser treatment of facial telangiectasia. *Dermatol Surg* 1998;24:71–74.
14. Dierickx CC, Farinelli WA, Anderson RR. Clinical and histological responses of blood vessels to long (msec) 532 nm laser pulses. *Lasers Surg Med* 1996;S(8):266.
15. Dierickx CC, Farinelli WA, Flotte T et al. Effect of long-pulsed 532 nm ND:YAG laser on port wine stains (PWS). *Lasers Surg Med* 1996;S(8):188.
16. Goldman MP, Eckhouse S. Photothermal sclerosis of leg veins. *Dermatol Surg* 1996;22:323–330.
17. Raulin C, Weiss RA, Schoenermark MP. Treatment of essential telangiectases with an intense pulsed light source (PhotoDerm VL®). *Dermatol Surg* 1997;23:941–946.
18. Raulin C, Schroeter C, Maushagen-Schnaas E. Einsatzgebiete einer hochenergetischen Blitzlampe (PhotoDerm VL). *Hautarzt* 1997;48:886–893.
19. Raulin C, Werner S, Hartschuh W, Schoenermark M. Effective treatment of hypertrichosis with pulsed light. A report of two cases. *Ann Plast Surg* 1997;39:169–173.
20. Raulin C, Hellwig S, Schoenermark MP. Treatment of a nonresponding port-wine stain with a new pulsed light source (PhotoDerm VL®). *Lasers Surg Med* 1997;21:203–208.
21. Maushagen-Schnaas E, Raulin C. Behandlung von benignen venösen Malformationen mit dem PhotoDerm VL. In: Garbe C, Rassner G, editors. *Dermatologie. Leitlinien und Qualitätssicherung für Diagnostik und Therapie. Berichte von der 39. Tagung der Deutschen Dermatologischen Gesellschaft*. New York: Springer; 1998. p 570–573.
22. Raulin C, Weiss RA, Schroeter CA, Keiner M, Werner S. Treatment of port wine stains with a non-coherent pulsed light source (PhotoDerm VL®)—A retrospective study. *Arch Dermatol* 1999; in press.
23. Schroeter CA, Wilder D, Reineke T, Thürlimann W, Raulin C, Neumann HAM. Clinical significance of an intense, pulsed light source on leg telangiectasias of up to 1 mm diameter. *Eur J Dermatol* 1997; 7:38–42.
24. Schroeter CA, Raulin C, Thürlimann W, Reineke T, de Potter O, Neumann M. Hair loss in 40 hirsute women with an intense light source, the PhotoDerm VL®. *Eur J Dermatol* 1999; in press.
25. Anderson RR, Parrish JA. Microvasculature can be selectively damaged using dye lasers: A basic theory and experimental evidence in human skin. *Lasers Surg Med* 1981;1:263–276.
26. Ashinoff R, Geronemus RG. Capillary hemangiomas and treatment with the flashlamp-pumped pulsed dye laser. *Arch Dermatol* 1991;127:202–205.
27. Alster TS, Wilson F. Treatment of port-wine stains with the flashlamp pumped dye laser: extended clinical experiences in children and adults. *Ann Plast Surg* 1994;32:478–484.
28. Tan OT, Murray S, Kurban AK. Action spectrum of vascular specific injury using pulsed irradiation. *J Invest Dermatol* 1989;92:868–871.
29. Anderson RR, Parrish JA. Selective photothermolysis: precise microsurgery by selective absorption of pulsed radiation. *Science* 1983;220:524–527.
30. Gemert van MJC, Welch AJ, Pickering JW, Tan OT, Gijssbers GHM. Wavelengths for laser treatment of port wine stains and telangiectasia. *Lasers Surg Med* 1995; 16:147–155.
31. Garden JM, Tan OT, Kerschmann R. Effect of dye laser pulse duration on selective cutaneous vascular injury. *J Invest Dermatol* 1986;87:653–657.
32. Dierickx CC, Casparian JM, Venugopalan V, Farinelli WA, Anderson RR. Thermal relaxation of port-wine stain vessels probed in vivo: The need for 1–10-ms laser pulse treatment. *J Invest Dermatol* 1995;105:709–714.
33. Kimel S, Svaasand LO, Hammer-Wilson M, Schell MJ, Milner TE, Nelson JS, Berns MW. Differential vascular response to laser photothermolysis. *J Invest Dermatol* 1994;103:693–700.
34. Goldman MP, Fitzpatrick RE. Treatment of cutaneous vascular lesions. In: Goldman MP, Fitzpatrick RE, editors. *Cutaneous laser surgery*. St. Louis: Mosby; 1994. p 19–105.
35. Apfelberg DB, Maser MR, White DN. Benefits of contact and noncontact YAG laser for periorbital hemangiomas. *Ann Plast Surg* 1990;24:397–408.
36. Apfelberg DB, Maser MR, White DN, et al. Combination treatment of massive cavernous hemangioma of the face: YAG laser photocoagulation plus direct steroid injection following by YAG laser resection with sapphire scalpel tips, aided by superselective embolization. *Lasers Surg Med* 1990;10:217–223.
37. Apfelberg DB, Lane B, Marx MP. Combined (team) approach to hemangioma management: arteriography with superselective embolization plus YAG laser/sapphire-tip resection. *Plast Reconstr Surg* 1991;88:71–82.
38. Apfelberg DB. Argon and YAG laser photocoagulation and excision of hemangiomas and vascular malformations of the nose. *West J Med* 1995;163:122–127.
39. Garden JM, Bakus AD. Laser treatment of port-wine

- stains and hemangiomas. *Dermatol Clinics* 1997;15(3): 373–383.
40. Foster TD, Gold MH. The successful use of the Photoderm VL® in the treatment of a cavernous hemangioma in a dark-skinned infant. *Min Invas Surg Nurs* 1996;10(3): 102–104.
41. Jay H, Borek C. Treatment of a venous-lake angioma with intense pulsed light. *The lancet* 1998;351,Jan. 10: 112.
42. Raulin C, Raulin SJ, Hellwig S, Schoenermark MP. Treatment of benign venous malformations with an intense pulsed light source (PhotoDerm VL®): report of two cases. *Eur J Dermatol* 1997;7:279–282.
43. Morelli JG, Weston WL, Huff JC, Yohn JJ. Initial lesion size as a predictive factor in determining the response of port-wine stains in children treated with the pulsed dye laser. *Arch Pediatr Adolesc Med* 1995;149(10):1142–1144.
44. Green D. Photothermal removal of telangiectases of the lower extremities with the Photoderm VL®. *J Am Acad Dermatol* 1998;38:61–68.
45. Tan OT, Sherwood K, Gilcrest BA. Treatment of children with port-wine stains using the flashlamp-pulsed tunable dye laser. *N Engl J Med* 1989;320:416–421.
46. Renfro L, Geronemus RG. Anatomical differences of port-wine stains in response to treatment with the pulsed dye laser. *Arch Dermatol* 1993;129:182–188.
47. Boixeda P, Núñez M, Pérez B, de las Heras ME, Hilara Y, Ledo A. Complications of 585-nm pulsed dye laser therapy. *Int J Dermatol* 1997;36:393–397.
48. Seukeran DC, Collins P, Sheehan-Dare RA. Adverse reactions following pulsed tunable dye laser treatment of port wine stains in 701 patients. *Br J Dermatol* 1997;136: 725–729.
49. Goldman MP, Fitzpatrick RE, Ruiz-Esparza J. Treatment of port-wine stains (capillary malformation) with the flashlamp-pumped pulsed dye laser. *J Pediatr* 1993; 122:71–77.
50. Taieb A, Touti L, Cony M, Leaute-Labreze C, Mortureux P, Renaud P, Boineau D, Malleville J. Treatment of port-wine stains with the 585-nm flashlamp-pulsed tunable dye laser: A study of 74 patients. *Dermatology* 1994;188: 276–281.
51. Haedersdal M, Efsen J, Gnieadecka M, Fogh H, Keiding J, Wulf HC. Changes in skin redness, pigmentation, echostructure, thickness, and surface contour after 1 pulsed dye laser treatment of port-wine stains in children. *Arch Dermatol* 1998;134:175–181.